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<p>(54) Title: RADIATION DETECTOR ARRAY USING RADIATION SENSITIVE BRIDGES</p>			
<p>(57) Abstract</p> <p>An infrared (IR) simulator is disclosed in which an array of pixels is defined on an insulative substrate by resistor bridges which contact the substrate at spaced locations and are separated from the substrate, and thereby thermally insulated therefrom, between the contact locations. Semiconductor drive circuits on the substrate enable desired current flows through the resistor bridges in response to input control signals, thereby establishing the appropriate IR radiation from each of the pixels. The drive circuits and also at least some of the electrical lead lines are preferably located under the resistor bridges. A thermal reflector below each bridge shields the drive circuit and reflects radiation to enhance the IR output. The drive circuits employ sample and hold circuits which produce a substantially flicker-free operation, with the resistor bridges being impedance matched with their respective drive circuits. The resistor bridges may be formed by coating insulative base bridges with a resistive layer having the desired properties, and overcoating the resistive layers with a thermally emissive material. The array is preferably formed on a silicon-on-sapphire (SOS) wafer. Arrays of electromagnetic radiation bridge detectors may also be formed, with the bridges having either resistor, thermocouple or Schottky junction constructions.</p>			

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RADIATION DETECTOR ARRAY USING RADIATION SENSITIVE BRIDGES

BACKGROUND OF THE INVENTION

Field of the Invention

This invention relates to systems for simulating an infrared image for use in testing infrared seekers. It also relates to detector arrays for electromagnetic radiation including infrared and microwave.

Description of the Related Art

It would be highly desirable to be able to simulate a real-time infrared (IR - roughly 0.7-20 microns wavelength) image that is substantially free of flicker. This would provide an effective way to test IR detectors, also referred to as "seekers" and "focal plane arrays". At present, problems of excessive flicker impose a serious constraint on IR simulation systems. A basic problem with image flicker is that it creates a false target indication, since flicker corresponds to a change in the temperature of the IR image. Unlike the human eye which integrates light flicker over a period of about 30-50 msec., IR detectors integrate flickers over periods of only about 1-5 msec. Thus, there is a significant range over which flicker (in the visible spectrum) would not be detected by the human eye but would be picked up by an IR detector if it is within the IR spectrum.

Excessive flicker has been avoided heretofore with the use of a Bly cell to project a static image that has been applied to the cell. Bly cells are described in Vincent T.

5 Bly, "Passive Visible to Infrared Transducer for Dynamic Infrared Image Simulation", Optical Engineering, Nov./Dec. 1982, Vol. 21, No. 6, pp. 1079-1082. However, the requirement that this type of system be operated with a static image is a significant limitation, since a more meaningful test of IR detectors calls for the detection of images that can change in real-time.

10 A prior attempt to produce an IR simulation system with a real-time image involved the formation of a video image by a cathode ray tube (CRT). The CRT video image was applied as an input to a liquid crystal light valve (LCLV), to which an IR readout beam was applied. The LCLV modulated the IR readout beam with the video image from the CRT to produce a corresponding IR video image. See S.T. Wu et al.,
15 "Infrared Liquid Crystal Light Valve", Proceedings of the SPIE, Vol. 572, pages 94-101, August, 1985.

20 This approach unfortunately was found to result in a substantial amount of flicker. The problem is that the illuminated pixels on the CRT screen decay in intensity over time prior to the next electron beam scan. This causes an undesirable intensity gradient to appear on a projected IR image from an IR-LCLV which is coupled to the CRT, and an IR detector will then detect a non-uniform image. Because the detector is generally looking for intensity gradients, or edges, by which its associated algorithms determine the presence of "targets", such intensity gradients are misleading. While this problem could theoretically be solved by synchronizing the IR detector scan with the CRT electron beam scan, such synchronization may
25 not be desired in many applications. Thus, although an IR-LCLV has the capability of projecting high resolution, high dynamic range, real-time simulated IR images when compared to a Bly cell, this advantage is mitigated by the CRT pixel decay. Furthermore, electrically driven matrix emitter devices have flicker if driven with simple RC-type pixel
30
35

addressing circuits, since the RC decay is similar in effect to the phosphor decay of the CRT.

Modifications of the basic CRT-LCLV system described above might be envisioned to reduce or eliminate flicker, but they introduce other problems. In one such modification, two storage CRTs are provided with shutters in front of each screen. Operation is alternated between the two CRTs by means of the shutters, so that they are alternately applied to the LCLV. By staggering the video data frames between the two CRTs, the phosphor decay seen by the LCLV could theoretically be reduced significantly. However, in such a system, it may be difficult to implement the very fast shutter coordination that would be necessary to substantially avoid flicker. Furthermore, storage CRTs are non-uniform, resulting in image differences and consequent flicker.

Another approach would be to use a single CRT, but to increase the frame rate of the Raster scan from the conventional rate of about 30 Hz to a much higher rate, perhaps about 1,000 Hz. The CRTs of the future may provide higher bandwidths than that presently attainable, thereby making this approach more attractive.

A possible approach which does not provide real-time addressable images is the use of a "flicker-free" film or slide projector like the SCANAGON® device produced by Robert Woltz Associates, Inc. of Newport Beach, California and disclosed in Patent Nos. 4,113,367 and 4,126,386, or a comparable image projector. While the potential may exist for this limited technique, it has not been demonstrated to provide jitter-free and flicker-free images. Furthermore, this method will not provide real-time electronically updatable imagery.

In addition to flicker-free images, it is very important for an IR simulation system to achieve high spatial resolution, large dynamic temperature ranges and fast res-

ponse. Spatial resolutions should be at least 500x500 pixels, with flicker less than 1%. For some applications frame rates should be 100 Hz or greater, and the dynamic thermal range should ideally be from near room temperature
5 (some applications require cooled background temperatures) to 1,000°C, particularly in the 3-5 micron spectral range. This combination of dynamic range and response time requirements is difficult for commercially available liquid crystals to achieve. Furthermore, most IR simulation
10 applications require the simulator to be mounted on the two-axis target arm of a Carco table, which is then moved relative to the IR seeker being tested. For this purpose weight and size limitations are very important. The liquid crystal based IR simulator requires a large blackbody source,
15 typically in excess of 100 pounds, and an expensive wire grid polarizer to be mounted with the active matrix. This reduces the mobility of the supporting Carco table arm.

Liquid crystal systems are also limited in dynamic
20 range because it is difficult to photogenerate enough charge in the silicon substrate, while maintaining spatial resolution, to rotate the liquid crystal molecules completely. Furthermore, there is a restriction on the speed of response of liquid crystals if a reasonable thermal dynamic range is to be maintained. The flicker problem associated with liquid crystal systems can be reduced by utilizing a flicker-free visible addressing source for the liquid crystal light valve. However, known sources of this type are limited in speed, resolution, weight and size.
25

30 Patent No. 4,724,356 to Daehler discloses a resistor-based IR simulator in which an array of resistors are individually addressed to stimulate IR emission. The Daehler approach is also discussed in Daehler, "Infrared Display Array", SPIE Vol. 765, Imaging Sensors and Displays (1987),
35 pages 94-101 and Burriesci et al., "A Dynamic RAM Imaging

Display Technology Utilizing Silicon Blackbody Emitters",
5 SPIE Vol. 765, Imaging Sensors and Displays (1987), pages
112-122. Both the resistors and their respective drive
transistor circuits are formed from a bulk silicon wafer.
10 An air gap groove is formed under the resistors to help
reduce thermal conduction losses to the underlying bulk
silicon wafer. To facilitate the selective etching used to
form the insulating air gap grooves, the top layer of the
15 wafer is heavily doped. However, this doping makes the top
layer electrically conductive, resulting in a significant
impedance mismatch between the resistors and their respec-
tive transistor drive circuits. As a result, most of the
input power is lost in the drive circuitry, rather than
going into IR radiation. This reduction in the power
transfer to the resistors results in a need for even more
15 input power to the transistors, leading to a potential
overheating problem.

In addition to an inefficient use of input power, in
20 the Daehler approach only a relatively small portion of the
pixel area (less than 10%) is actually occupied by the
radiating resistor. Much of the area that might otherwise
be devoted to the resistor is occupied by the drive trans-
istors and the insulating air gap. As a result, to achieve
25 a given apparent temperature for the pixel as a whole the
resistor itself must be heated to a significantly higher
temperature. This substantially reduces the system's
effective thermal dynamic range.

Another problem with the Daehler approach relates to
30 the electrical lead lines used to address the individual
pixels. Relatively large silicon wafers must be used with
present technology to achieve a significant number of pix-
els. For example, a wafer of about four inches is required
for a 512x512 array. This means that the electrical lead
35 lines on the chip must also be about four inches long.
This in turn leads to two significant problems. First,

there is a large amount of capacitive coupling associated with the long lead lines. Parasitic capacitance between conductive substrate and metal lead lines can limit the response time. Second, defects such as pin holes can appear in the oxide insulator formed on the substrate, causing a short circuit between the line and the silicon substrate which renders the associated pixel or pixels inoperative. The longer the lines, the greater is the probability of such defects. Daehler tries to resolve this problem by limiting the size of the array to 8x128 pixels, and coupling many such arrays together side-by-side to produce an aggregate array of reasonable size. However, the coupling process itself introduces significant complexities.

There is also a need for a two-dimensional IR detector array, and for detector arrays at other electromagnetic radiation (emr) wavelengths such as microwave, which have a fast response and make efficient use of available area.

Various types of IR thermal detectors are currently available. In pyroelectric detectors, a temperature change alters the dipole moment of the material, resulting in a charge difference between crystal faces. This type of detector is discussed in an article by Watton, "Ferroelectrics for Infrared Detection and Imaging", Proceedings of the Sixth IEEE International Symposium on the Application of Ferroelectrics, June 1986, Bethlehem, Pennsylvania, pages 172-181. Another type of IR detector is the bolometer, in which the energy of absorbed radiation raises the temperature of the detecting element to change its electrical resistance, which change is measured as an indication of the amount of received radiation. An array of such devices is disclosed in Boninsegni et al., "Low Temperature Bolometer Array", Review of Scientific Instruments, Vol. 60, No. 4, April 1989, pages 661-665. Both the pyroelectric and bolometer devices exhibit a relatively slow rate

of response to changes in IR level, and also require relatively large areas. The pyroelectric thermal detector also suffers from limited resolvable temperature differences, low yield and high cost processing, a necessary hybrid integration and AC operation with a chopper. The limited temperature resolution, which is principally due to the inherent thermal conduction loss and large thermal mass, can be improved by thinning and reticulating the pyroelectric wafer, but this involves very difficult and expensive processing.

Another approach to IR detection involves an array of single crystal Schottky junctions, as disclosed in Tsaur et al., "IR Si Schottky-Barrier Infrared Detectors With 10- μm Cutoff Wavelength", IEEE Electron Device Letters, Vol. 9, No. 12, December 1988, pages 650-653. This device is used as a photon detector rather than a thermal detector, has a very limited spectral range, and has to be operated at cryogenic temperatures.

Thermocouple devices provide another IR thermal detector. In this type of device junctions are formed between dissimilar materials, with a voltage induced across the junction in response to heating. Such a device is disclosed in Lahiji et al., "A Batch-Fabricated Silicon Thermopile Infrared Detector", IEEE Transactions on Electron Devices, Jan. 1982, pages 14-22. In this article a series of thermocouples have hot junctions which are supported on a thin silicon membrane by integrated circuit techniques. The membrane area is coated with a layer of IR absorbing material to efficiently absorb energy from the visible to the far infrared. The sensitivity of the device is limited because the thermocouples are formed directly on the substrate and therefore cannot heat as much as desired due to the thermal conduction losses. Also, a relatively large area is required for the detector.

5 Bolometers and crystal detectors have also been used to sense emr at microwave frequencies. Since relatively large sensor dimensions are necessary, single detectors have been used to scan an incoming image, rather than using a detector array to sense the entire image at one time. The result has been slow frame rates. The same problem has attended the use of single scanning junction detectors in the IR require.

10 SUMMARY OF THE INVENTION

15 In view of the above problems, the goal of the present invention is to provide an IR simulation system which is substantially flicker-free, light in weight, has a large thermal dynamic range and fast response, is power efficient, devotes most of the pixel area to the radiating element, and avoids the capacitive coupling and insulator defect problems associated with long lead lines on a single crystal semiconductor substrate. A two-dimensional emr detector array with similar characteristics is also includ-
20 ed.

25 This goal is achieved in accordance with the invention by providing an IR pixel matrix in the form of an array of resistor bridges formed on an insulating substrate, such as sapphire. The resistor bridges span a portion of each pix-
30 el cell, contact the substrate at spaced-apart contact locations, and are shaped to form a thermally insulative gap between the bridge and substrate. A semiconductor drive circuit on the substrate enables a desired amount of current flow through the bridge in response to an input control signal to heat the bridge, thereby producing a desired amount of IR radiation. Control, actuating and power lead lines extend along the substrate to deliver control and actuating signals to the drive circuits, and an elec-
 trical power signal to the resistor bridges; since the sub-

strate is insulative, capacitive coupling and shorting problems are mitigated even with long lead lines.

In the preferred embodiment the drive circuits are located on the substrate surface under the resistor bridges, and at least some of the lead lines also extend under the bridges. Each pixel cell includes a thermally reflective element between the resistor bridge and drive circuit to reflect IR radiation away from the drive circuit. The thermally reflective element may comprise either a second bridge formed from a thermally reflective material which bridges the drive circuit and is spaced from both that circuit and the resistor bridge, or a thermally reflective layer which overlies an insulative layer on the drive circuit.

To reduce flicker to less than 1%, the drive circuit for each pixel comprises a sample and hold circuit in which a first transistor applies a control signal to a holding capacitor, and a second transistor applies a power signal to the resistor bridge in response to the capacitor signal. The electrical impedance of the resistor bridge preferably matches that of the drive circuit.

The resistor bridges may be implemented in various ways. In one implementation they comprise a base bridge formed from an insulative material, with a resistive layer over the base. The resistivity and thickness of the resistive layer are selected to produce a desired resistance. The resistive layer may itself be surmounted by a coating of high thermal emissive material. The resistor bridge may also be formed from a material having an enhanced porosity which decreases its thermal conductivity. To concentrate the voltage drops towards the centers of the bridges and away from their connections with the substrate, the bridges may be tapered so that their cross-sectional areas near the center are significantly less than near their contacts with the substrate.

The resulting IR pixel array has a significantly better combination of thermal dynamic range, speed of response, resolution, weight, size, efficiency and flicker-free operation than any other known system. The invention 5 also includes two-dimensional emr sensing arrays consisting of an array of emr detector cells formed on a substrate. Each cell includes an emr sensitive bridge structure. The shape of the bridge structure is designed to form a generally insulative gap between the bridge and the substrate. 10 The bridge structure has a defined characteristic which varies with the amount of received emr, and means are provided for monitoring this characteristic for each of the cells to determine the level of emr incident on each cell.

The bridge structures can be implemented by resistor 15 bridges, thermocouple junction bridges, or Schottky junction bridges. With resistor bridges, various bridge geometries may be selected to reduce the area of the bridge support legs relative to the center span, and thereby assist in thermally insulating the center span from the substrate. Multiple-stage amplifier readout circuits are 20 preferably employed in connection with output voltage divider circuits to monitor the effective bridge resistances with a reduced Johnson noise. Thin layers of conductive material may be added to the support legs to electrically connect the center span to the underlying monitoring circuits, the conductive material layers being thin enough to substantially maintain the thermal isolation of the bridge center spans from the substrate. The resistor bridges are 25 preferably formed from an amorphous semiconductor material.

With a thermocouple bridge detector array, the thermocouples 30 preferably comprise a stacked plurality of alternating semiconductor and metal layers. The junction devices are connected in series with resistors and output voltage divider circuits, with the voltages across the output

resistors monitored as a function of the emr received by the thermocouple bridges.

The Schottky junction bridge embodiment employs a bridge configured as adjacent layers of a semiconductor material and a metal or doped semiconductor, meeting along a Schottky contact junction. The semiconductor is preferably amorphous germanium or amorphous tin.

The detector bridges are preferably coated with a layer of emr absorbing material to increase their sensitivity. Readout circuits for each detector cell are preferably located on the substrate at least partially under their respective bridges to conserve substrate area. Various lead lines may also extend under the bridge structures to further conserve substrate area. A lens is employed to image an emr source onto the two-dimensional array. Additional features and advantages of the invention will be apparent to those skilled in the art from the following detailed description of preferred embodiments, taken together with the accompanying drawings, in which:

DESCRIPTION OF THE DRAWINGS

FIG. 1 is a block diagram of an IR simulator system which incorporates the present invention;

FIG. 2 is a diagrammatic plan view of a portion of the pixel cell array used to create an IR image;

FIG. 3 is a schematic diagram of the drive circuitry employed in each pixel cell;

FIGS. 4-6 are sectional views showing different embodiments of the resistor bridge which provides the IR radiating element for each pixel;

FIGS. 7-9 are sectional views illustrating various embodiments of the relationship between the resistor bridge of each pixel and the drive circuitry therefore;

FIG. 10 is an illustrative plan view showing the disposition of electrical lead lines with respect to the re-

sistor bridge for one embodiment;

FIG. 11 is a sectional view of a resistor bridge emr detector and readout circuit in accordance with the invention;

5 FIGs. 12(a), 13(a) and 14(a) are plan views and FIGs. 12(b), 13(b) and 14(b) are front elevation views of three different resistor bridge configurations which thermally isolate the center span of the bridge from the underlying substrate;

10 FIG. 15 is a simplified schematic diagram of a readout circuit for a resistor bridge emr detector;

FIG. 16 is a more complete schematic diagram of the circuit shown in FIG. 15;

15 FIG. 17 is a sectional view showing the formation of a transistor and capacitor of FIG. 16 in a single monolithic construction;

FIG. 18 is a schematic diagram of another readout circuit for a bridge resistor emr detector which reduces Johnson noise;

20 FIG. 19 is a sectional view of a thermocouple bridge emr detector;

FIG. 20 is a simplified schematic diagram of a readout circuit for the detector of FIG. 19;

25 FIG. 21 is a sectional view of a Schottky junction bridge emr detector;

FIG. 22 is a simplified schematic diagram of a readout circuit for the emr detector of FIG. 21; and

30 FIG. 23 is a block diagram showing the imaging of an emr source onto a detector array constructed in accordance with the invention.

DETAILED DESCRIPTION OF THE INVENTION

35 FIG. 1 shows the basic elements of an IR simulation system constructed in accordance with the invention. An IR radiating mechanism 2 is placed within a vacuum chamber

4 which has an IR window 6 at its forward end. A vacuum pump 8 evacuates the chamber in a conventional manner. The IR structure includes an insulative substrate 10, preferably sapphire, a two-dimensional array 12 of IR emitting elements on the forward side of substrate 10, and a cooling mechanism 14 contacting the rear of the substrate. The cooling element is preferably a copper block cooled by water or freon flowing through inlet and outlet pipes 16. The IR window 6 is formed from a suitable material such germanium or zinc selinide, and is preferably provided with an anti-reflective coating to prevent reflection of emitted IR radiation back into the chamber.

The individual IR emitting elements within the array 12 provide controlled emissions which are directed by a lens 18 onto an IR detector 20 being tested. The emissions from each individual IR radiating element are controlled by electrical signals applied to the array. The electrical leads into the array include a power line 22 connected to a DC power source, a series of data lines 24 which carry image information signals to the various IR elements, a series of strobe lines 26 which strobe rows of IR elements in succession in coordination with the image signal, and a ground line 28. The image data input signals may represent an actual video image, a computer simulation, or other desired pattern.

The IR radiating array is divided into a matrix of pixel cells, each of which is individually controlled to emit a desired amount of IR radiation. The resolution of the IR image is governed by the number of pixels, which are typically provided in a 256x256, 512x512 or 1024x1024 array. A section of such an array is illustrated in FIG. 2. Each pixel cell includes a resistor bridge 30, which is the actual IR radiating element, and a drive circuit 32 for the resistor bridge. Each pixel cell is typically about 150 microns square, while the resistor bridges are

about 120 microns square. The drive circuits employ two transistors, each of which is typically about 50 microns square. The aluminum electrical lead lines are typically about 25 microns wide.

5 FIG. 2 is a simplified drawing which illustrates the functional relationship between the various elements in the array, but does not show them in their preferred physical arrangement; this will be discussed further below. One end of each resistor bridge 30 is connected to a DC power line 22, while the other end is connected to its associated 10 drive circuit 32. Each drive circuit acts in response to an applied image signal from line 24 to control the flow of current from the power line, through the resistor bridge and drive circuit to ground.

15 The pixel cells are arranged in a matrix of rows and columns. Electrical inputs are provided in a manner that allows each pixel to be separately programmed, yet avoids the need for separate lead lines for each pixel. Discrete signals are applied to the line 24 for each column, so that 20 each drive circuit in a given column receives the same signal, but the signals vary from column-to-column. Each row of pixel cells is strobed in succession via strobe lines 26, which are connected to the pixel drive circuits. The application of a strobe signal enables the operation of a 25 drive circuit, which otherwise holds off the flow of any current through the resistor bridge. By varying the pattern of image data signals in synchronism with the progression of the strobe signal from row-to-row, a unique signal can be applied to each pixel cell to establish the resistor current through that cell at a unique value. The drive 30 circuits are designed so that they can acquire an image data signal only during the brief period when the circuit is being strobed, so that the changing pattern of signals while other rows are being strobed has no effect upon the 35 signal acquired by a particular pixel. Each drive circuit

includes a sample and hold circuit which holds the acquired image data signal during the period of time required to strobe all of the other rows. With a frame rate in the order of 100 Hz, the sample and hold circuits keep the decay of the video signals acquired by their respective pixels to less than 1%. This results in a substantially flicker-free operation.

A schematic diagram of the preferred drive circuit for each pixel is given in FIG. 3. The circuit is preferably implemented with a silicon-on-sapphire (SOS) wafer in which the active circuit elements are formed from a silicon layer 12 on the sapphire substrate 10. SOS wafers are currently available in 5 inch diameters, and larger wafers will probably be produced in the future. Since an insulating substrate is employed, the prior problem of shorting and capacitive coupling from the lead lines is substantially eliminated, thereby permitting the use of large arrays.

Each sample and hold circuit includes a first FET T1 with its source-drain circuit connecting the image data input to a holding capacitor C1. The signal held by C1 is applied to the gate of a second FET T2, and controls the amount of current flow permitted by T2. The bridge resistor 30 is connected between the DC power source and the drain or source of T2, depending upon the transistor connection; the opposite source-drain terminal of T2 is connected to ground. Thus, the amount of current permitted to flow through resistor 30, and accordingly the amount of IR radiation emitted by resistor 30, is controlled by the video signal held by C1 and applied to the gate of T2.

A simple implementation of bridge resistor 30 is shown in FIG. 4. The resistor has a center span 34 that is elevated above the surface of sapphire substrate 10 by a pair of legs 36 at opposite ends of the center span. The vertical air gap clearance between center span 34 and the substrate is preferably about 2-5 microns, which is sufficient

to prevent substantial thermal conduction loss from the resistor to the substrate. The method of forming such a bridge resistor is known, and is described in Patent No. 4,239,312 to Myer et al., assigned to Hughes Aircraft Company, the assignee of the present invention. The bridge resistor could also be implemented with electrically conductive, metallic vertical legs and a planar center span of resistor material. In this configuration, because the legs have high electrical conductivity, there is a proportionate reduction in the voltage-induced thermal gradients, and reduction in stress.

Whereas the resistors employed in the Daehler IR simulator were limited to boron doped silicon because of the bulk silicon substrate, with the present invention the resistor material can be selected to optimize its characteristics. Ideally, the resistor should have a low thermal conductivity to limit heat transfer to the substrate, an electrical conductivity which matches the resistor impedance to the impedance of the drive circuit, a low coefficient of thermal expansion to prevent the resistor from expanding significantly with respect to the lower temperature substrate, and a high melting point. One suitable resistor material is polysilicon, which has a high melting temperature, controllable resistivity, small temperature dependent resistivity, and a low coefficient of thermal expansion. Other materials which may be suitable include graphite, which has good temperature properties, high emissivity, titanium oxides, tantalum oxides, silicon oxides and cermets.

To minimize thermal stress at the junction between the bridge resistor and the substrate, the bridge may be fabricated as shown in FIG. 5 so that its legs 36 are relatively thick where they contact the substrate, and progressively taper in cross-sectional area towards the center span 34. This arrangement reduces the resistance of the legs, parti-

cularly in the vicinity of the substrate, and also adds mechanical support. Accordingly, the bulk of the voltage drop and the resultant high temperature will occur at the center span 34, which is desirable to both reduce mechanical stress and enhance IR radiation. The temperature of the bridge will be lower along its legs, particularly near the substrate, since less power is dissipated there.

Further protection against heat loss may be obtained by increasing the porosity of the resistor material through electron beam deposition or other suitable technique. An increased porosity reduces the thermal conductivity of the material, making it even less susceptible.

In another embodiment, illustrated in FIG. 6, the resistor bridge is formed from a base bridge 38 of insulative material such as SiO_2 , with a thin resistive layer 40 over the base bridge 38. The resistivity and thickness of the resistive layer 40 are selected to produce the desired resistance for the bridge. A very thin metal or ceramic-metal (cermet) layer, preferably on the order of about 50 Angstroms thick, would be suitable. The insulative base bridge 38 should itself be made as thin as possible, consistent with the required mechanical support, to provide fast response and low thermal conductivity. SiO_2 about 0.5-1 micron thick would be suitable. The resistive layer 40 might be coated with a layer of high thermal emissive material 42, such as carbon black or gold black, to improve the radiative efficiency of the bridge. The thermally emissive layer may then be sealed with a sealing coat of SiO_2 about 50-100 Angstroms thick.

To preserve space on the substrate and free up more area for the resistor bridges, the drive circuits 32 are preferably located under the bridges, as illustrated in FIG. 7. To maintain the drive circuitry at reasonable operating temperatures, it may be shielded from the heat of the resistor by means of a second bridge 44 as illu-

strated in FIG. 8. This second bridge is spaced from both the resistor bridge 30 and the drive circuit 32, and is formed from a thermally reflective material such as aluminum. In addition to protecting the circuit elements from overheating, the reflective bridge 44 increases the pixel output power, since most of the IR radiation which it reflects is transmitted through the thin resistor bridge to enhance the output IR radiation.

FIG. 9 illustrates an alternate to the discrete reflective bridge 44. In this embodiment an electrically insulative layer 46 such as SiO_2 is laid down over the drive circuit 32, followed by a thermally reflective layer 48 such as aluminum over the insulative layer.

Additional area on the array may be conserved and devoted to the radiating resistor elements by directing at least some of the lead lines under the bridge resistors. Such an arrangement is illustrated in FIG. 10. In this single layer metallization scheme, the image data, power and ground lines for each pixel 50 are run under the resistor bridge 30, while the strobe line extends along the side of the resistor. With a double layer metallization, all four lines could be separated by insulating layers and run under the bridge. Single and double layer metallization techniques are well known in the art. For further savings in real estate, adjacent pixels could share the same power and ground lines.

The preferred technique for fabricating the array is to first fabricate the drive circuits on an SOS wafer. The whole substrate is then covered with a spacer layer, such as potassium chloride or aluminum, which can be selectively etched. A resist layer is then laid on top of the spacer layer to define the pixels. The resist at the intended resistor bridge locations is next exposed, the unexposed resist is washed off, and the spacer layer below the removed resist is etched away. After removing the remaining

resist the bridge material is overcoated on the remaining spacer layer by a technique such as sputtering or electron beam evaporation, depending upon the bridge material and properties desired. A shadow mask technique might also be employed to form the bridges, but it is difficult to obtain desirably high pixel density and small bridge dimension with this technique. Finally, the remaining spacer material is removed by standard techniques, such as dissolving away potassium chloride or etching away aluminum.

With the described IR simulation system, 60-65% of the pixel area can be devoted to the resistor. As a result, the resistors do not need to be heated to as high a temperature to attain a given effective pixel temperature as with the prior system that employed much smaller resistors. The resistors can be tailored to impedance match the drive circuits, thereby significantly improving the efficiency of the device. The problems of capacitive and electrical shorting associated with the lead lines is also substantially alleviated. The device is calculated to have an effective thermal dynamic range of 1,000°C in the 3-5 micron region, and 600°-700°C in the 8-12 micron region (with the substrate at room temperature). Frame rates of 200 Hz are achievable without bothersome flicker.

The bridge structure of the present invention can also be used as a sensitive and space-efficient emr detector for IR, microwave and other wavelengths. A particular range of wavelengths can be selected for sensing by an appropriate selection of the bridge dimensions, generally following the rule that the length of the bridge should be at least half the desired wavelength. IR wavelengths are quite small, so the bridges in this range will generally be considerably larger than a half wavelength. Microwave wavelengths are much longer, on the order of cms., so microwave detector bridges would not need to be much bigger than a half wavelength. With the use of a refractive lens or, in the case

of microwaves, a focusing reflector, the emr beam can be at least partially focused to permit the use of smaller detector bridges.

FIG. 11 illustrates a resistance bridge detector that can be used for this purpose. The bridge 52 consists of a center span 54 with support legs 56 at either end extending up from a substrate 57, and a readout circuit 58 on the substrate under the chip and at least partially shaded thereby from incident emr.

A preferred material for the bridge is amorphous silicon, which has a relatively high temperature coefficient of resistance, is compatible with integrated circuit processing, and can be formed with controlled mechanical stresses. Other amorphous semiconductors are also suitable, such as Ge, SiGe, and SiC. Materials which are generally unsuitable for the resistor bridge include metals because of high thermal conductivity and a low electrical resistance and low temperature coefficient of resistance, insulators because of low conductivity, and cermets because of low temperature coefficients of resistance. The substrate 57 is preferably single crystal silicon for relatively small dimensions in the IR regime, or a silicon-on-insulator construction for larger microwave dimensions.

A layer 60 of an emr absorbent material, such as metallic black or black paint for IR, is provided on the bridge center span, which is the emr target area, to increase the emr-induced temperature variation. Various geometric configurations for the bridge can also be designed to assist in thermally isolating the center span from the substrate, and thereby increase the potential degree of heating for the center span and thus the device's sensitivity. This goal may be accomplished by making the cross-sectional areas of the legs which support the center span much less than the area of the center span emr target area. In FIGs. 12(a) and 12(b) the center span 54a is rectangu-

lar, while a pair of support legs 56a extend from opposite sides of the center span and are quite narrow where they meet the center span. The support legs broaden out to the same width as the center span along the substrate to provide a more secure bridge retention. By contrast, in FIGS. 5 13(a) and 13(b) the center span 54b has the same rectangular configuration, but the support legs 56b consist of narrow tabs 56b at each corner of the center span. In FIGS. 10 14(a) and 14(b) the center span 56 has a generally serpentine configuration to increase its effective length, and thereby enhance its thermal isolation, by increasing the length of the average thermal path between the center span and the substrate. Support legs 56c consist of narrow tabs at opposite ends of the center span.

15 A thin metal layer, typically on the order of 100 Angstroms thick, is established over each of the support legs to provide an electrical shunt between the center span and the underlying readout circuit. This significantly reduces I²R heating in the legs. Because they are so thin, the metal layers themselves do not conduct heat significantly.

20 FIG. 15 is a simplified schematic diagram of an output circuit that can be used to monitor the bridge resistance of each detector cell, and thereby the level of emr received by that cell. Similar readout circuits would be replicated for each of the individual cells. The circuit consists of a basic voltage divider formed by the variable bridge resistance R_b in series with a load resistor R_L. Positive and negative bias voltages V_b are applied across the series network, while the output at the midpoint of the 25 two resistors is amplified by an amplifier A1 and delivered as an output voltage V_o. Any emr-induced change in R_b will alter the bridge circuit, and adjust V_o accordingly.

30 A computer model has been devised to estimate the performance of a thin amorphous silicon bridge detector of this type. The resulting estimation for the bridge respon-

sivity to applied emr in a vacuum is 4×10^3 volts/watt, for an amorphous silicon bridge having a thermal conductivity of about $0.0256 \text{ J/cm} \cdot ^\circ\text{K}$, a temperature coefficient of 2%, a resistivity of 100 ohm-cm, dimensions of $100 \times 40 \times 1$ microns, and a bias voltage V_b of 5 volts. Assuming Johnson (or resistive) noise is a limiting source of noise figure, the estimated noise equivalent power is near $3.4 \times 10^{-10} \text{ W}$, and the corresponding detectivity is $1.8 \times 10^8 \text{ cm} - \text{Hz}^{0.5}/\text{W}$ for an effective bandwidth of 100 Hz. The minimum resolvable temperature difference at 300°K background is then close to 0.17°C , and the total power consumption for a 320×160 detector array is on the order of 2 Watts. This estimated performance is quite suitable for applications of an uncooled IR imaging system.

A more detailed schematic of an output circuit for each resistor bridge detector is provided in FIG. 16. Resistors R1 and R2 are chosen to maximize the product of the transistor transconductance and output resistances. The upper transistor T2 provides a large dynamic load, but relatively low static load, for the bottom amplifying transistor T1, resulting in a large gain.

Since the detector array will have a large number of output circuits of this type, one for each bridge detector, the output circuits are arranged in a matrix configuration with a strobe signal S applied to an output transistor T3 to obtain an output from each individual readout circuit at a desired strobe time. A capacitor C across the drain and gate of amplifier transistor T1 provides a large equivalent capacitance, and a corresponding low level of Johnson noise; the strobe readout process via T3 also discharges (resets) capacitor C. The equivalent capacitance of the circuit is given by the expression $C(1+A)$, where A is the amplifier gain.

A physical construction by which T1 and C can be monolithically integrated into the same structure is shown in

FIG. 17. A gate metallization 58 is formed over an oxide layer 60 on the substrate, with a heavily doped semiconductor layer 62 underlying a portion of metallization 58 and oxide 60, and extending laterally to one side. A gate connection is made to metallization layer 58, a drain connection is made to doped semiconductor layer 62, and a source connection is made to a heavily doped region 64 on the opposite side of oxide layer 60 from drain layer 62. The transistor channel comprises the portion of the substrate between drain 62 and source 64, while capacitor C is established by the aligned portions of gate metallization 58 and drain layer 62.

While the provision of a large equivalent capacitance in the circuit of FIG. 16 produces a significant reduction in Johnson noise, it is still a limiting factor in the operation of the circuit. An alternate readout circuit is shown in FIG. 18 which further reduces the Johnson noise level. This circuit employs a two-stage amplifier, with the capacitor C connected across the second amplifier A2 and an input resistor R2 for A2. Johnson noise is reduced by a factor of $\sqrt{R_2/R_L}$. In addition, the capacitance of C can be reduced, with a corresponding reduction in the chip area required by the capacitor, to the extent the total amplification of the two-stage amplifier of FIG. 18 exceeds the amplification of the single-stage amplifier discussed above.

FIG. 19 shows a different form of bridge emr detector which, as with the resistance bridge detector discussed above, can be dimensioned to detect various emr wavelengths. The sensor is basically a thermocouple bridge 56 which generates a thermally induced voltage in response to received emr. It consists of a bridge structure with alternating layers of dissimilar materials. While in theory any two different materials could be used to produce a thermal junction voltage, metal-semiconductor junctions

have generally been found to produce the highest voltage levels. The bridge is preferably fabricated as a stacked layer, with thin metal layers 68 such as platinum alternating with semiconductor layers 70 such as amorphous SiGe. 5 The metal layers are preferably about 0.1-0.2 microns thick, while the semiconductor layers are about 0.5-2 microns thick to give sufficient mechanical strength. The thermocouple stack is surmounted by a heavily doped semiconductor back contact layer 72, which in turn is capped by 10 a layer 74 of radiation absorbing material. The back contact layer 72 can be formed by a low energy ion implant to a depth on the order of 0.1 microns. An opening or "via" 76 is formed in the radiation absorbent coating 74 to provide a passage for an electrical lead line 78 to establish 15 contact with back contact layer 72. A readout circuit 80 is provided on the substrate, below and at least partially shaded by the bridge 66, to monitor the emr-induced thermocouple voltage.

A simplified schematic of a readout circuit for this 20 embodiment is given in FIG. 20. A load resistor R_L is connected in series with the thermocouple junction, represented as a variable voltage source 82. A bias voltage source 84 is connected across this voltage divider circuit, with the voltage V_0 across R_L monitored as an indication of the 25 emr-induced voltage across the junction.

The detector array of the present invention can also 30 be implemented as a Schottky junction bridge 86, illustrated in FIG. 21. In this embodiment, a semiconductor layer 88 is formed over a bridge-shaped metal layer 90 to establish a Schottky junction. The semiconductor layer 88 should have a small bandgap to obtain a high leakage current across the junction, with a corresponding high sensitivity. Semiconductors such as amorphous germanium or amorphous tin are suitable for this purpose. A heavily 35 doped semiconductor that is substantially conductive can

also be used instead of metal layer 90. As with the thermocouple embodiment, the bridge is topped by a doped back contact layer 92 and a radiation absorbent layer 94, with a lead 96 electrically contacting the back contact through a via 98 in the radiation absorbent coating.

The readout circuit 100 for each bridge is again preferably located under the bridge, and at least partially shaded thereby. A simplified form of a suitable readout circuit is shown in FIG. 22. The Schottky junction bridge, represented by Schottky diode 102, is connected in series with a load resistor R_L . A voltage source 104 is connected across the series circuit to reverse bias the Schottky junction. Changes in the Schottky leakage current appear as an output voltage V_o across R_L , which is monitored as an indication of the emr incident on the bridge.

The detector bridges for each of the three embodiments, resistance, thermocouple and Schottky junction, are fabricated in a manner similar to the IR simulator bridge described previously. Spacer layers are established at the intended bridge locations, the bridges are formed over the spacer layers, and the spacer material is then dissolved or etched away.

An emr source 106 can be imaged onto an array 108 of the described emr detectors by placing a collimating lens 110 in the path of the emr travelling towards the detector array. While only a small number of individual detector bridges are shown on detector array 108 for simplicity, in practice the arrays would have a large number of individual bridge detectors. The actual number for any particular application would depend upon the required bridge dimensions for the radiation to be detected, the available dimensions for the overall array, and the desired resolution. An array of 320 X 160 individual detector elements might be typical.

In practice, the sensitivity of the resistance of the bridge resistor and that of the load resistor to variations in their dimensions, as well as variations in the output voltage of the pixel circuits due to nonuniformities in bias voltage and amplifier gains, makes it important to have an on-board compensation technique to correct for the resulting image nonuniformities. Because the dimensional changes are small and could in principle also be caused by mechanical and/or ambient thermal stresses, it is necessary to correct on a periodic basis. To correct for such non-uniformities, a shutter can be placed in front of the detector array and periodically closed to obtain a black readout. This readout is stored in a ROM or other convenient storage device, and used to compensate readouts with the shutter open. The system operation is preferably performed in an analog format, with the calibration information stored digitally. With a video sample rate of 30 frames per second, recalibration might be performed perhaps once an hour.

Electrical input and output lines can be conveniently run along the substrate, passing under the individual detector bridges to conserve substrate area, in a manner similar to that shown in FIGS. 2 and 10 for the IR simulator array. Power lines, ground lines, output lines and strobe lines would typically be employed.

Since numerous variations and alternate embodiments will occur to those skilled in the art, it is intended that the invention be limited only in terms of the appended claims.

WE CLAIM:

1. A two-dimensional sensing array for electromagnetic radiation (emr), comprising:

a substrate,

5 each of said cells including an emr sensitive bridge structure spanning a portion of the cell, said bridge structure being shaped to form a generally thermally insulative gap between the bridge structure and substrate, and having a defined characteristic which varies in accordance with the amount of emr received by the bridge, and

10 means for monitoring said defined characteristic for each of said cells.

2. The emr sensing array of claim 1, said bridge structures comprising respective resistor bridges.

3. The emr sensing array of claim 2, said resistor bridges comprising a center span having a target area for receiving emr and a plurality of support legs elevating the center span above the substrate, the geometries of said center span and support legs being selected to enhance emr absorption by the center span relative to thermal losses from the center span to the substrate through the support legs.

5. The emr sensing array of claim 3, wherein the cross-sectional areas of said support legs are substantially less than the areas of their respective target areas to thermally insulate the center span from the substrate.

4. The emr sensing array of claim 4, wherein a pair of support legs are provided for each center span, generally centered on opposite sides of the support span.

6. The emr sensing array of claim 4, said center spans generally comprising rectangles, wherein a support leg is provided adjacent each corner of said rectangles.

7. The emr sensing array of claim 3, said center spans having a generally serpentine configuration to increase their effective lengths and reduce thermal conduction losses therefrom.

5 8. The emr sensing array of claim 2, said monitoring means comprising respective resistors connected in series with the resistor bridges to form respective voltage divider circuits, means for applying a voltage to said voltage divider circuits, and means for monitoring the voltages across said resistors as a function of the emr received by said resistor bridges.

5 9. The emr sensing array of claim 8, said monitoring means comprising respective monitoring circuits at each cell, said monitoring circuits including multiple-stage amplifier readout circuits to reduce Johnson noise associated with said voltage divider circuits.

5 10. The emr sensing array of claim 2, said monitoring means including respective monitoring circuits at each cell, said resistor bridges comprising a center span having a target area for receiving emr, a plurality of support legs elevating the center span above the substrate, and a thin layer of conductive material on said support legs electrically connecting said center span to said monitoring circuits, said layers of conductive material being thin enough to substantially maintain the thermal isolation of said center spans from the substrate.

11. The emr sensing array of claim 2, said resistor bridges being formed from an amorphous semiconductor material.

5

12. The emr sensing array of claim 1, said bridge structures comprising respective junction devices having an electrical characteristic which varies in accordance with the amount of emr received by the junction device, and said monitoring means comprises means for monitoring said electrical characteristic for each of said cells.

5

13. The emr sensing array of claim 12, said junction devices comprising junctions of unlike materials selected to generate a thermally induced voltage, said junction devices being configured to heat in response to applied emr within a desired range of wavelengths, and said monitoring means comprises means for sensing thermally induced voltages in each of said junction devices.

14. The emr sensing array of claim 13, said junction devices comprising semiconductor-metal junctions.

15. The emr sensing array of claim 14, said junction devices comprising a stacked plurality of alternating semiconductor and metal layers.

5

16. The emr sensing array of claim 13, said monitoring means comprising respective resistors connected in series with said junction devices to form respective voltage divider circuits, means for applying a voltage to said voltage divider circuits, and means for monitoring the voltages across said resistors as a function of the emr received by said junction devices.

17. The emr sensing array of claim 12, said junction devices comprising Schottky diode bridge structures, and said monitoring means comprises means for reverse biasing said Schottky diode bridge structures and monitoring their leakage currents as a function of emr-induced heating.

5

18. The emr sensing array of claim 17, said Schottky contact bridge structures comprising adjacent layers of a semiconductor with a metal or doped semiconductor conductor, said layers meeting along a Schottky contact junction.

19. The emr sensing array of claim 18, wherein said semiconductor is amorphous germanium or amorphous tin.

5

20. The emr sensing array of claim 1, said emr sensitive bridge structures including a layer of emr absorbing material for receiving emr and activating the remainder of the bridge structures to vary said defined characteristic in response to emr received by said absorbing material.

5

21. The emr sensing array of claim 1, said monitoring means including a readout circuit for each cell situated on the substrate at least partially under the bridge structure for that cell and at least partially shaded thereby from applied emr.

5

22. The emr sensing array of claim 21, said monitoring means including actuating and monitoring lead lines extending along the substrate for respectively actuating the bridge structures response to received emr and monitoring said responses, at least some of said lines extending under at least some of said bridge structures.

23. The emr sensing array of claim 1, further including a lens for imaging an emr source onto said array.

24. An emr detector, comprising:

a substrate,

an emr bridge structure spanning a portion of said substrate and separated therefrom by a generally thermally insulative gap, said bridge structure having a defined characteristic which varies in accordance with the amount of emr which it receives,

means for elevating the bridge structures above the substrate, and

10 means for monitoring said defined characteristic.

25. The emr detector of claim 24, said bridge structure comprising a resistor bridge.

26. The emr detector of claim 25, said bridge structure and elevating means comprising a center span having a target area for receiving emr and a plurality of support legs elevating the center span above the substrate, the geometries of said center span and support legs being selected to enhance emr absorption by the center span relative to thermal losses from the center span to the substrate through the support legs.

5 27. The emr detector of claim 26, wherein the cross-sectional areas of said support legs are substantially less than the target area of said target area to thermally insulate the center span from the substrate.

28. The emr detector of claim 27, wherein a pair of support legs are provided for the center span, generally centered on opposite sides of the support span.

29. The emr detector of claim 27, said center span generally comprising a rectangle, wherein a support leg is provided adjacent each corner of said rectangle.

30. The emr detector of claim 26, said center span having a generally serpentine configuration to increase its effective length and reduce thermal conduction losses therefrom.

5

31. The emr detector of claim 26, said monitoring means including a monitoring circuit on the substrate, and further comprising a thin layer of conductive material on said support legs electrically connecting said center span to said monitoring circuit, said layers of conductive material being thin enough to substantially maintain the thermal isolation of said center span from the substrate.

5

32. The emr detector of claim 25, said monitoring means comprising a resistor connected in series with the resistor bridge to form a voltage divider circuit, means for applying a voltage to said voltage divider circuit, and means for monitoring the voltage across said resistor as a function of the emr received by the resistor bridge.

33. The emr detector of claim 32, said monitoring means including a multiple-stage amplifier readout circuit to reduce Johnson noise associated with said voltage divider circuit.

34. The emr detector of claim 25, said resistor bridge being formed from an amorphous semiconductor material.

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35. The emr detector of claim 24, said bridge structure comprising a junction device having an electrical characteristic which varies in accordance with the amount of emr received by the junction device, and said monitoring means comprises means for monitoring said electrical characteristic.

36. The emr detector of claim 35, said junction device comprising a junction of unlike materials selected to generate a thermally induced voltage and configured to heat in response to applied emr within a desired range of wavelengths, and said monitoring means comprises means for a thermally induced voltage in said junction device.

5

37. The emr detector of claim 36, said junction device comprising a semiconductor-metal junction.

38. The emr detector of claim 37, said junction device comprising a stacked plurality of alternating semiconductor and metal layers.

5

39. The emr detector of claim 36, said monitoring means comprising a resistor connected in series with said junction device to form a voltage divider circuit, means for applying a voltage to said voltage divider circuit, and means for monitoring the voltage across said resistor as a function of the emr received by the junction device.

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40. The emr detector of claim 35, said junction device comprising a Schottky diode bridge structure, and said monitoring means comprises means for reverse biasing said Schottky diode bridge structure and monitoring its leakage current as a function of emr-induced heating.

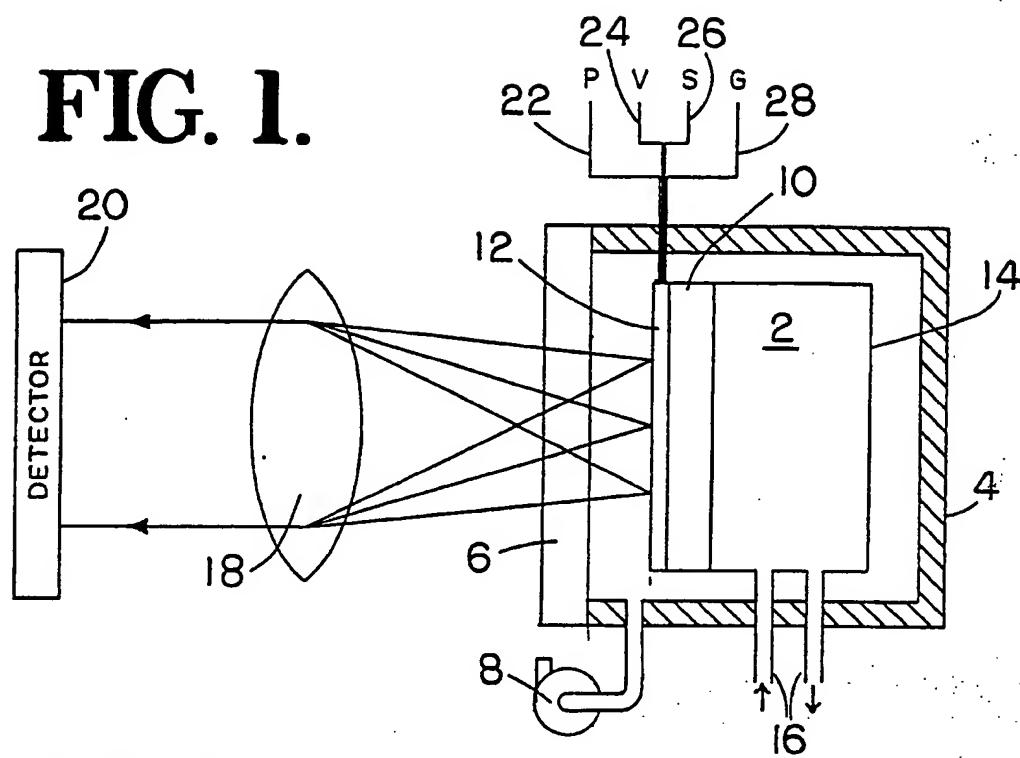
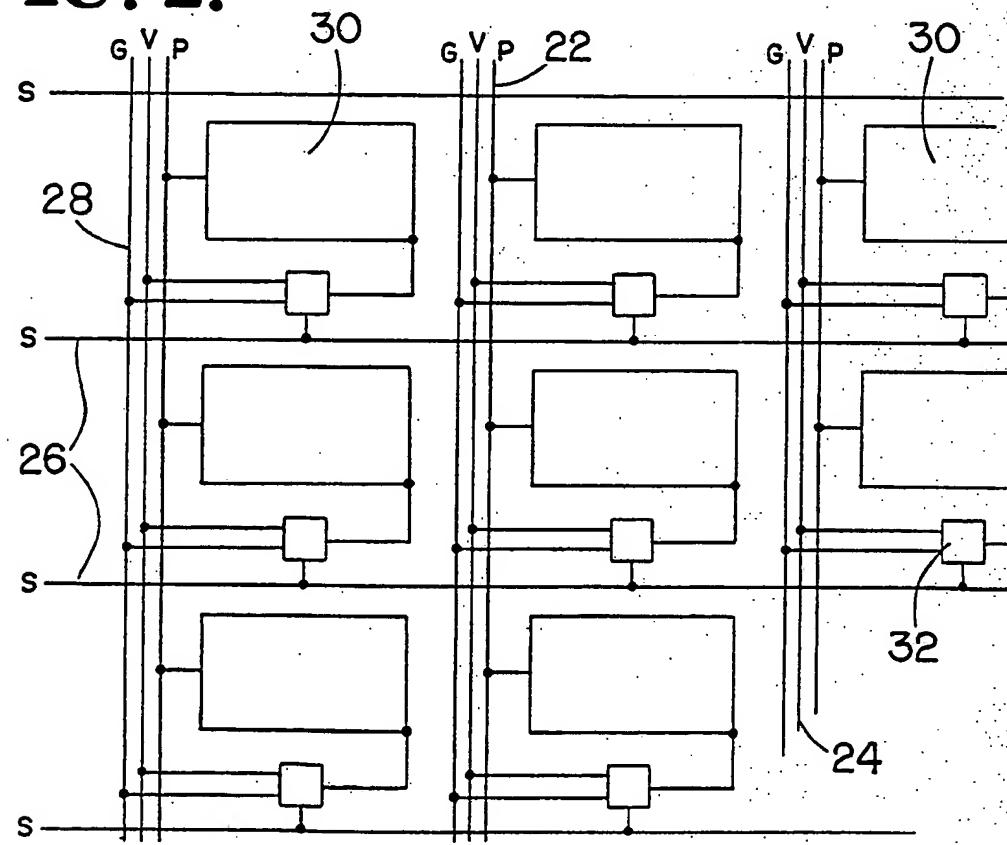
41. The emr detector of claim 40, said Schottky contact bridge structure comprising adjacent layers of a semiconductor with a metal or doped semiconductor conductor, said layers meeting along a Schottky contact junction.

42. The emr detector of claim 41, wherein said semiconductor is amorphous germanium or amorphous tin.

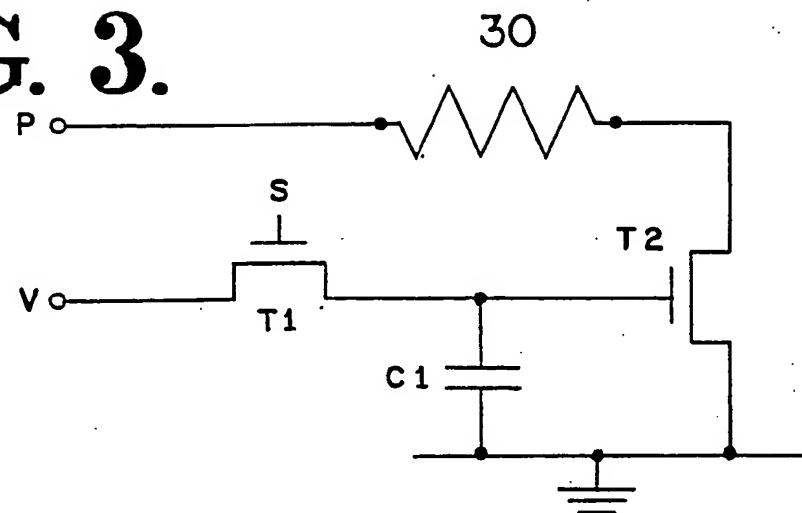
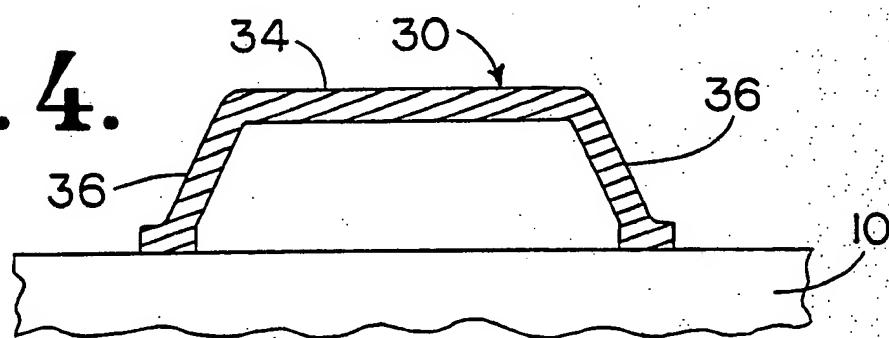
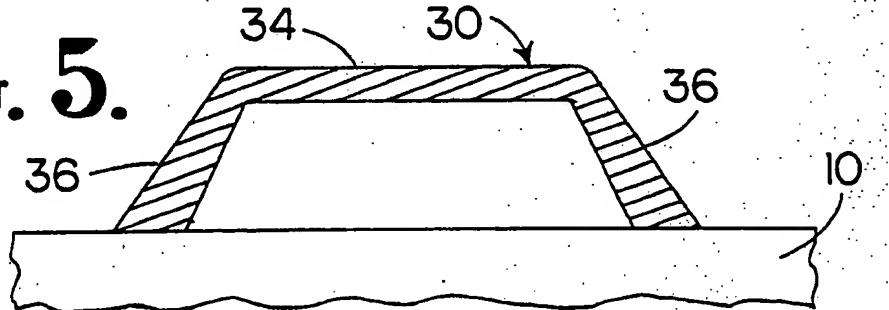
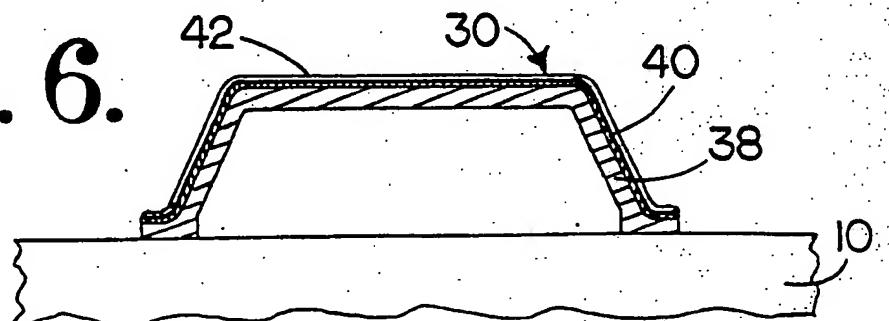
43. The emr detector of claim 24, said emr sensitive bridge structure including a layer of emr absorbing material for receiving emr and activating the remainder of the bridge structures to vary said defined characteristic in response to emr received by said absorbing material.

5 44. The emr detector of claim 24, said monitoring means including a readout circuit situated on the substrate at least partially under said bridge structure and at least partially shaded thereby from applied emr.

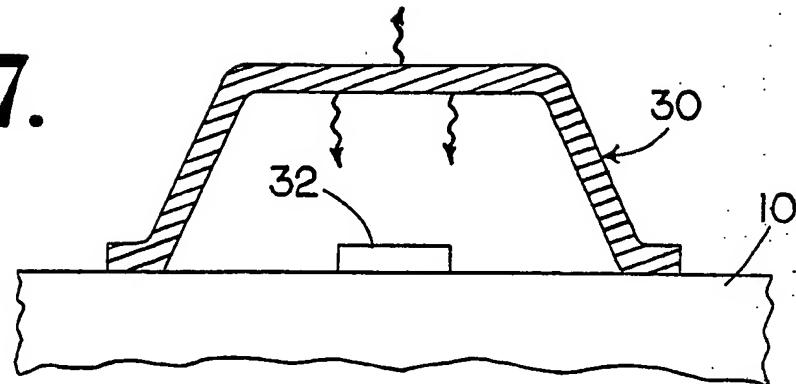
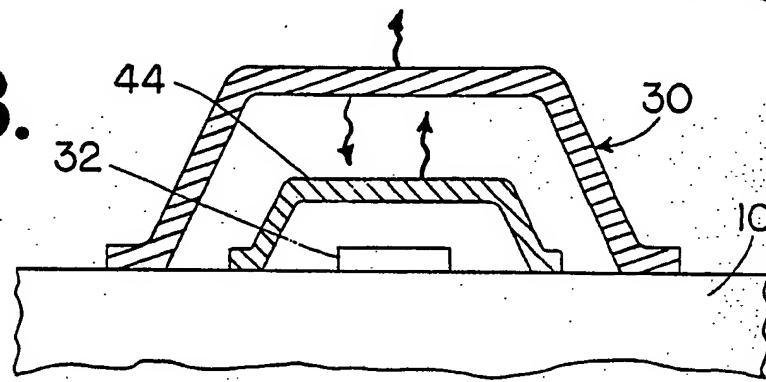
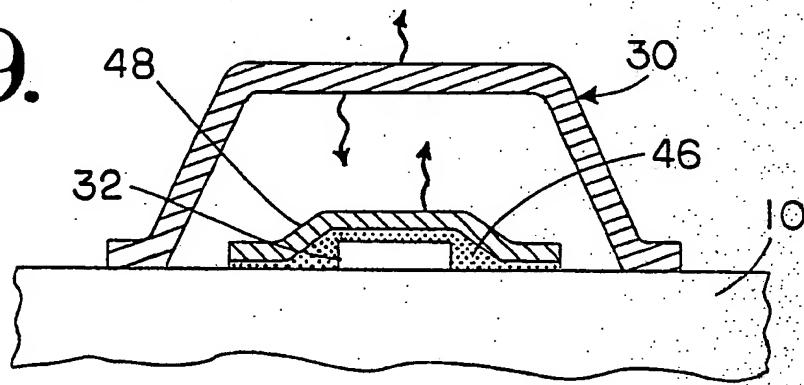
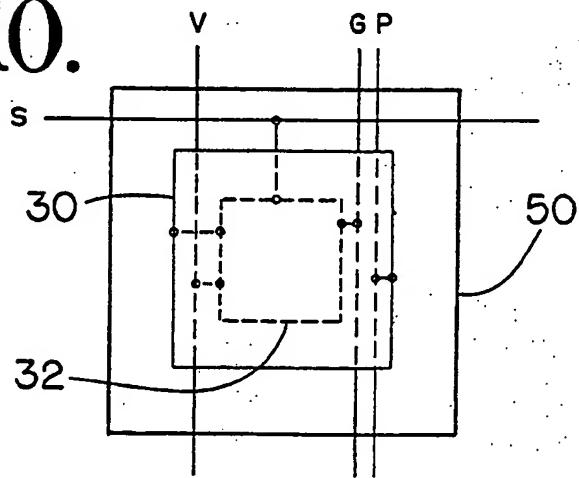
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FIG. 1.**FIG. 2.**

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FIG. 3.**FIG. 4.****FIG. 5.****FIG. 6.**

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FIG. 7.**FIG. 8.****FIG. 9.****FIG. 10.**

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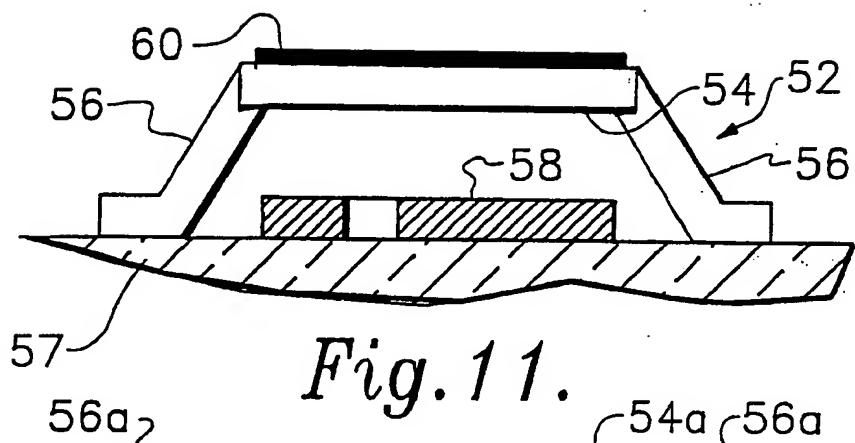


Fig. 11.

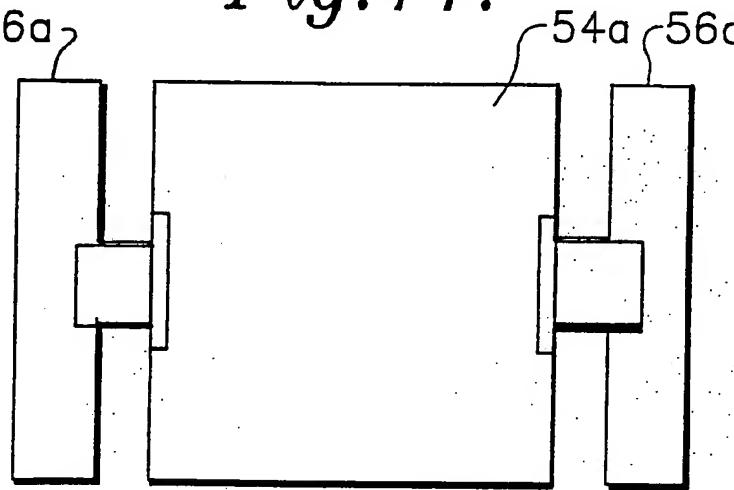


Fig. 12.a.

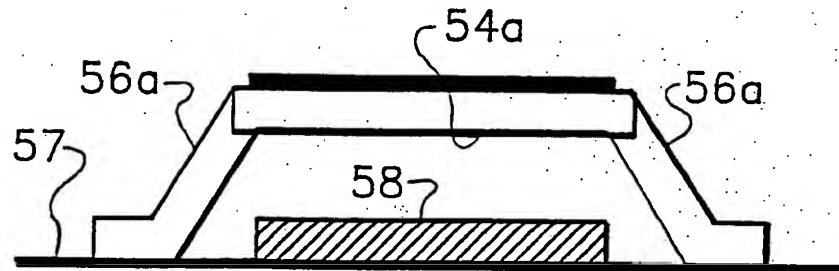


Fig. 12.b.

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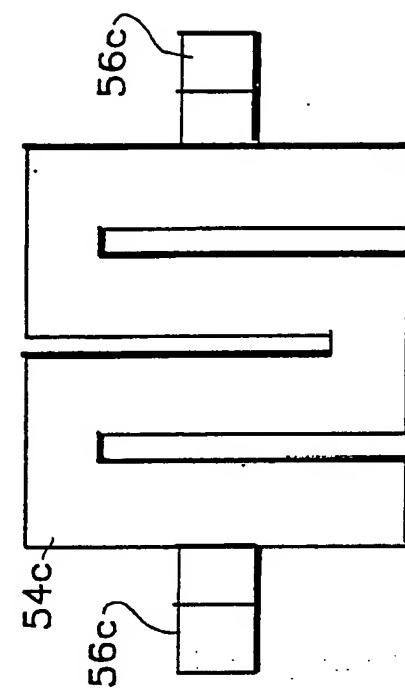


Fig. 14.a

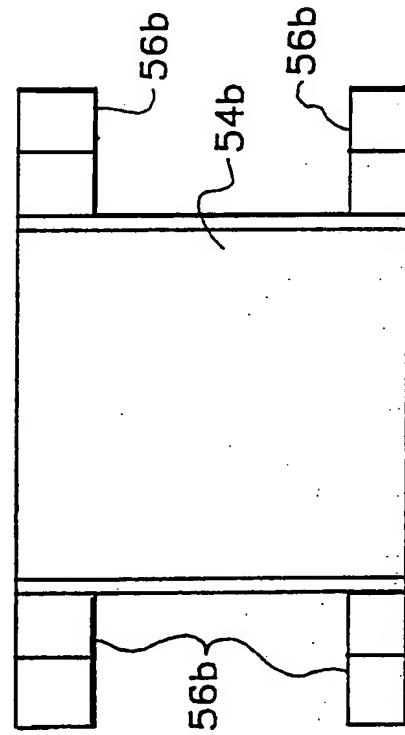


Fig. 13.a.

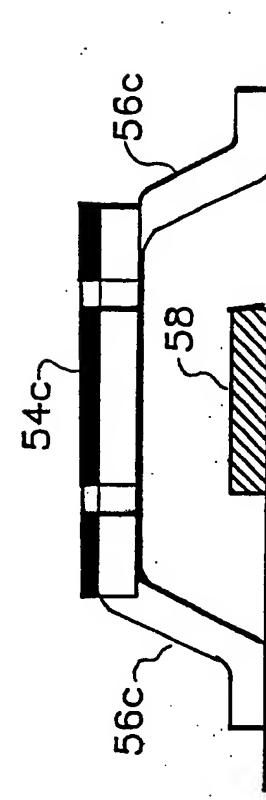


Fig. 14.b.

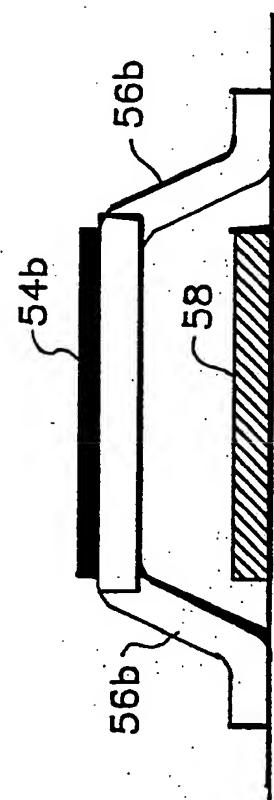


Fig. 13.b

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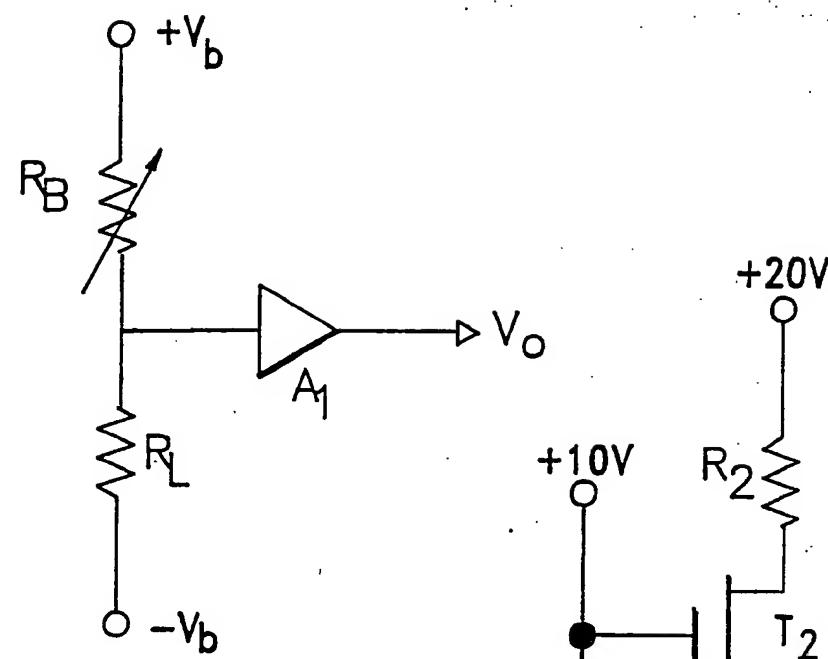


Fig. 15.

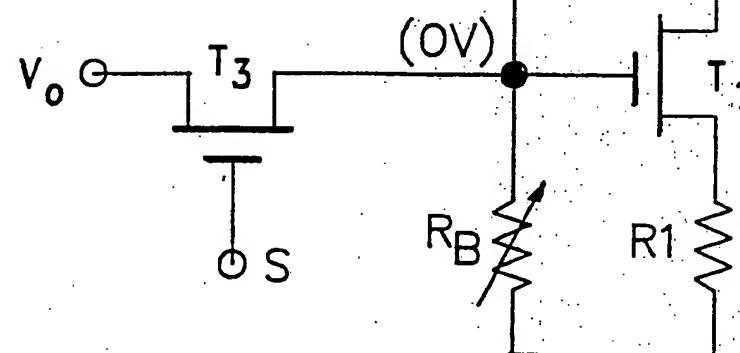


Fig. 16.

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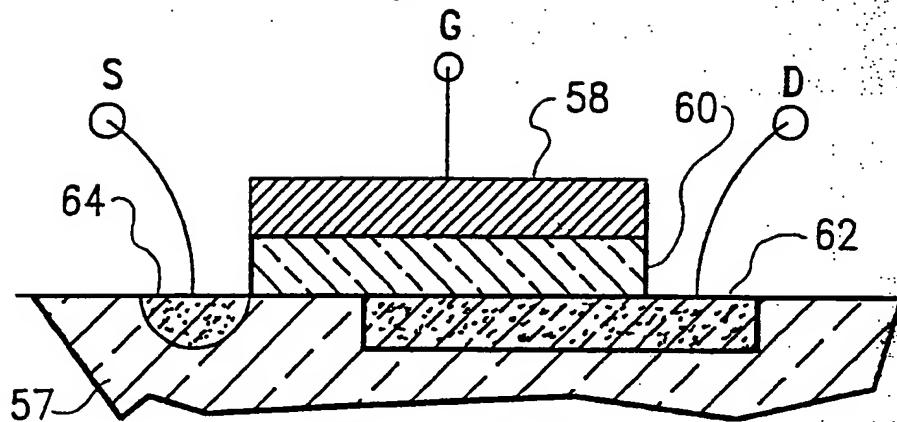


Fig. 17.

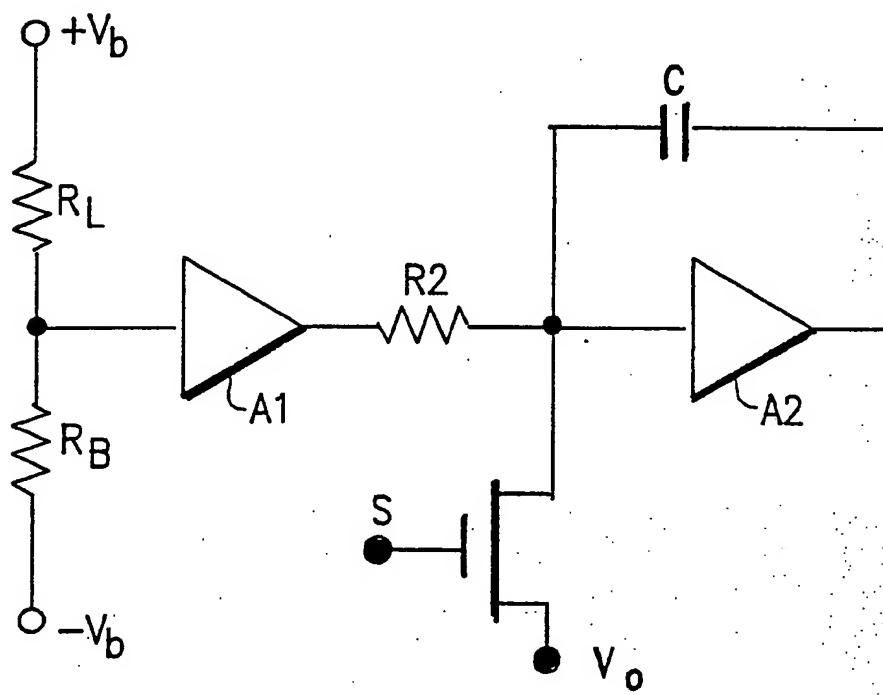


Fig. 18.

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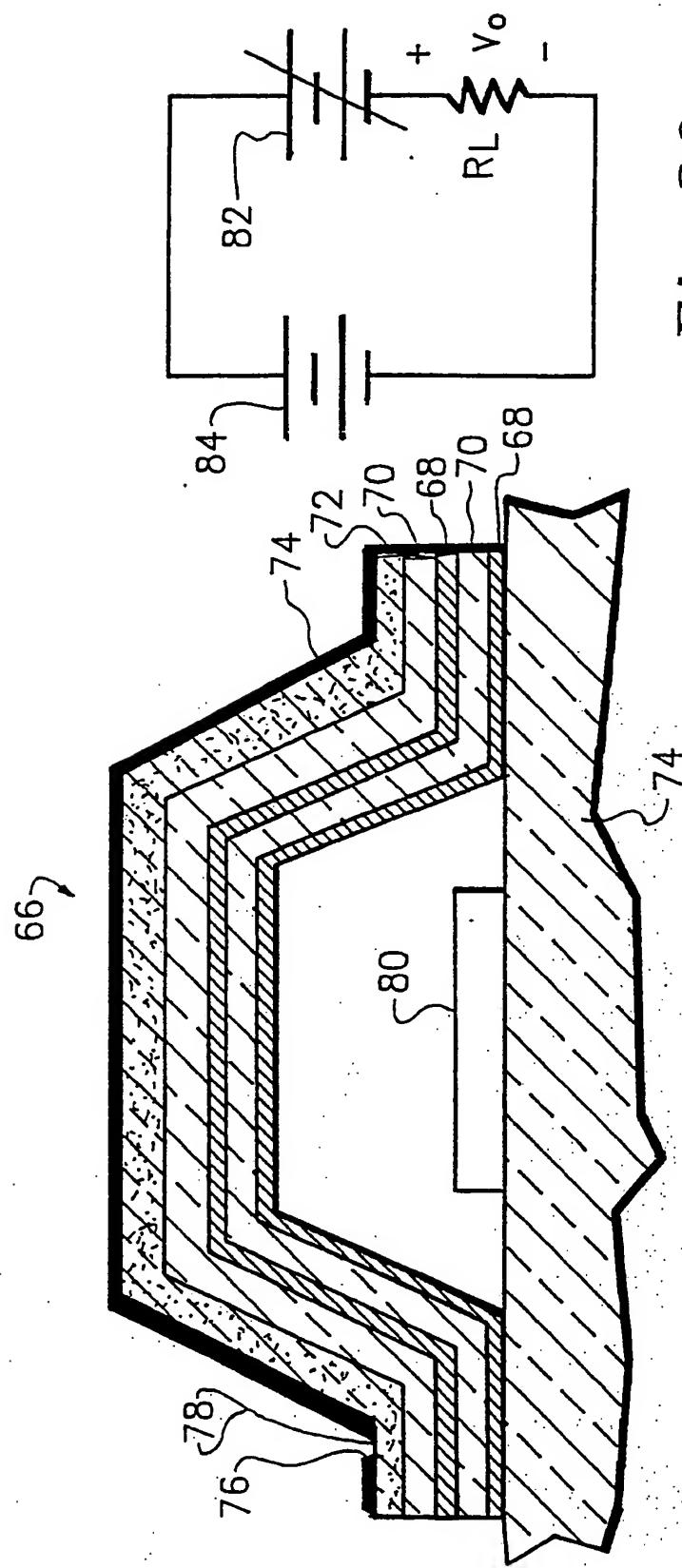


Fig.20.

Fig.19.

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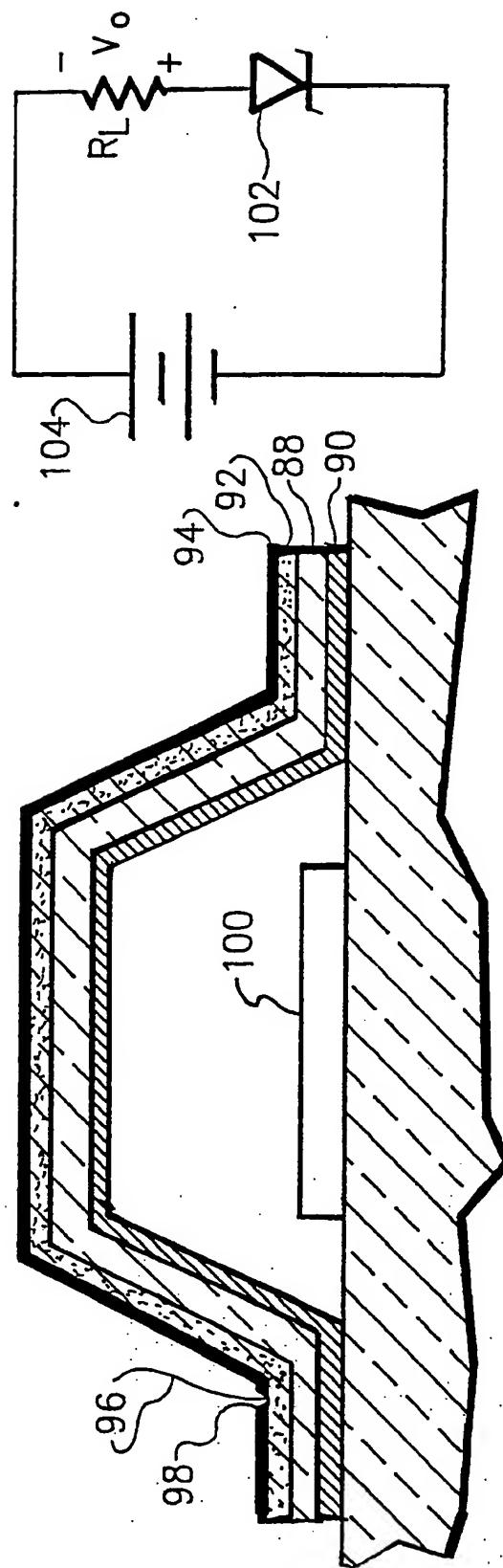


Fig. 22.

Fig. 21

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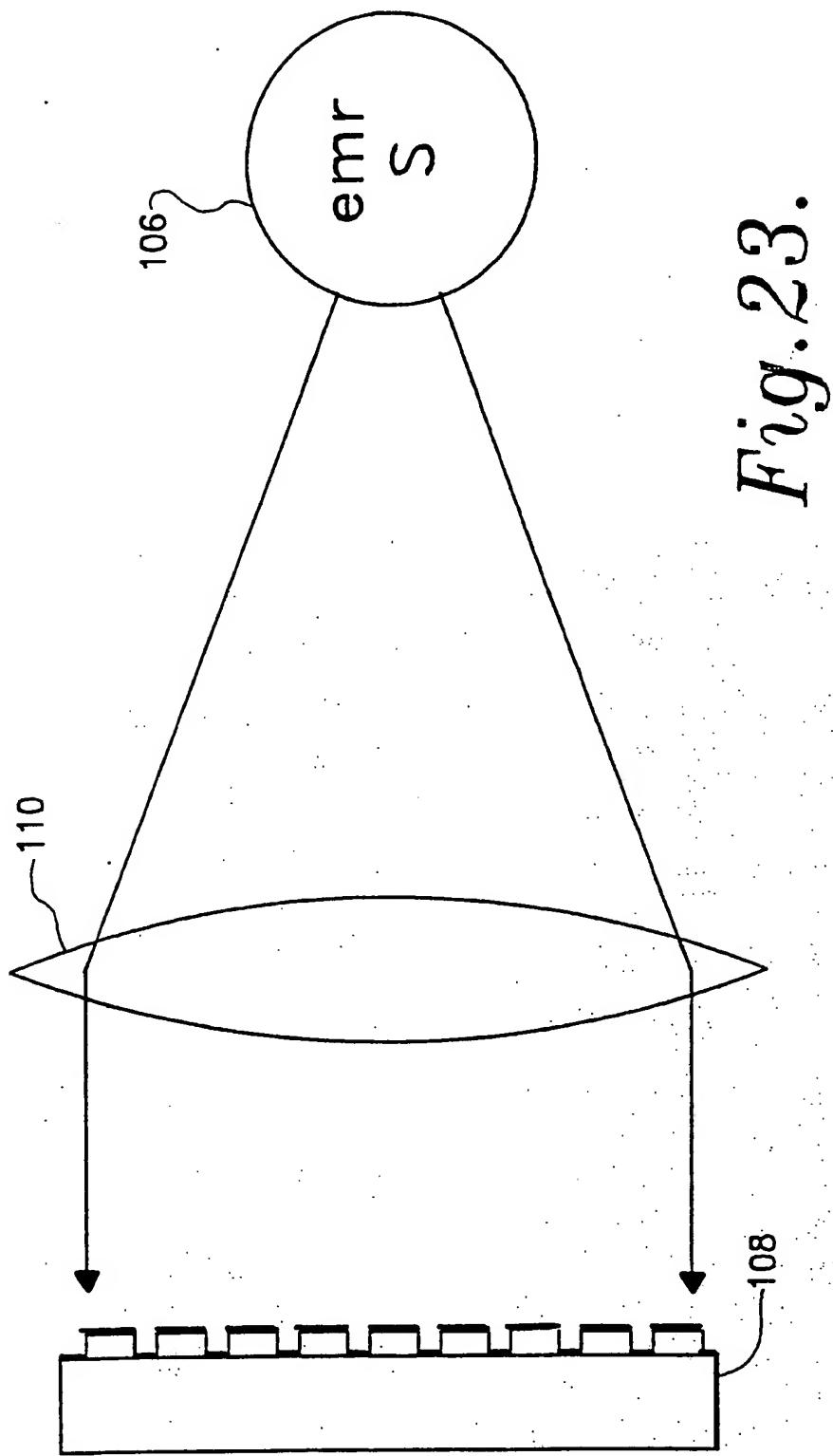


Fig. 23.

INTERNATIONAL SEARCH REPORT

International Application No. PCT/US 90/00525

I. CLASSIFICATION OF SUBJECT MATTER (If several classification symbols apply, indicate all) *

According to International Patent Classification (IPC) or to both National Classification and IPC

IPC⁵: H 01 L 27/146, G 01 J 5/20

II. FIELDS SEARCHED

Minimum Documentation Searched ?

Classification System	Classification Symbols
IPC ⁵	H 01 L, G 01 J

Documentation Searched other than Minimum Documentation
to the Extent that such Documents are Included in the Fields Searched *

III. DOCUMENTS CONSIDERED TO BE RELEVANT*

Category *	Citation of Document, ¹¹ with indication, where appropriate, of the relevant passages ¹²	Relevant to Claim No. ¹³
X	DE, A, 3240180 (SIEMENS) 3 May 1984 see abstract; page 9, line 30 - page 13, line 8; figures	1, 24
Y	--	2-5, 8, 20, 23, 25-28, 32, 43
Y	US, A, 4463262 (CONTRERAS) 31 July 1984 see column 2, line 50 - column 6, line 5; figures	2-5, 8, 25-28, 32
A	--	9, 11, 21, 33, 34, 44
Y	FR, A, 2570494 (INTERNATIONAL STANDARD ELECTRIC CORPORATION) 21 March 1986 see page 3, lines 6-8; figure 1	20, 43
	--	. / .

* Special categories of cited documents: ¹⁰

- "A" document defining the general state of the art which is not considered to be of particular relevance
- "E" earlier document but published on or after the international filing date
- "L" document which may throw doubt on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

"A" document member of the same patent family

IV. CERTIFICATION

Date of the Actual Completion of the International Search

27th September 1990

Date of Mailing of this International Search Report

24.10.90

International Searching Authority

EUROPEAN PATENT OFFICE

Signature of Authorized Officer

M. Peis

M. PEIS

III. DOCUMENTS CONSIDERED TO BE RELEVANT (CONTINUED FROM THE SECOND SHEET)

Category *	Citation of Document, ¹¹ with indication, where appropriate, of the relevant passages	Relevant to Claim No.
Y	DE, A, 3411186 (BATTELLE-INSTITUT) 10 October 1985 see page 6, last paragraph; figure 1 --	23
A	US, A, 4544441 (HARTMANN) 1 October 1985 see column 4, lines 54-62; figures --	7, 30
X	DE, A, 3240180 (SIEMENS) 3 May 1984 see the whole document	12, 35
Y	--	13, 14, 17, 18, 36, 37, 40, 41
Y	IEEE Transactions on Electron Devices, volume ED-29, no. 1, January 1982, IEEE, (New York, US), G.R. Lahiji et al.: "A batch-fabricated silicon thermopile infrared detector", pages 14-22 see the whole article	13, 14, 36, 37
A	(cited in the application) --	15, 38
Y	IEEE Electron Device Letters, volume 9, no. 12, December 1988, IEEE, (New York, US), B.-Y Tsaur et al.: "IrSi Schottky- Barrier infrared detectors with 10 ⁻⁷ μm cutoff wavelength", pages 650-653 see abstract; page 650, paragraphs 1-3	17, 18, 40, 41
A	(cited in the application) -----	19, 42

FURTHER INFORMATION CONTINUED FROM THE SECOND SHEET

V. OBSERVATIONS WHERE CERTAIN CLAIMS WERE FOUND UNSEARCHABLE¹

This International search report has not been established in respect of certain claims under Article 17(2) (a) for the following reasons:

1. Claim numbers because they relate to subject matter not required to be searched by this Authority, namely:

2. Claim numbers because they relate to parts of the International application that do not comply with the prescribed requirements to such an extent that no meaningful International search can be carried out, specifically:

3. Claim numbers....., because they are dependent claims and are not drafted in accordance with the second and third sentences of PCT Rule 6.4(a).

VI. OBSERVATIONS WHERE UNITY OF INVENTION IS LACKING²

This International Searching Authority found multiple inventions in this International application as follows:

1. Claims : 1 - 11, 20 -34, 43, 44
2. Claims : 12 - 19, 35 - 42,

1. As all required additional search fees were timely paid by the applicant, this International search report covers all searchable claims of the international application.

2. As only some of the required additional search fees were timely paid by the applicant, this International search report covers only those claims of the International application for which fees were paid, specifically claims:

3. No required additional search fees were timely paid by the applicant. Consequently, this International search report is restricted to the invention first mentioned in the claims; it is covered by claim numbers:

4. As all searchable claims could be searched without effort justifying an additional fee, the International Searching Authority did not invite payment of any additional fee.

Remark on Protest

The additional search fees were accompanied by applicant's protest.

No protest accompanied the payment of additional search fees.

**ANNEX TO THE INTERNATIONAL SEARCH REPORT
ON INTERNATIONAL PATENT APPLICATION NO.**

**US 9000525
SA 35172**

This annex lists the patent family members relating to the patent documents cited in the above-mentioned international search report. The members are as contained in the European Patent Office EDP file on 15/10/90. The European Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
DE-A- 3240180	03-05-84	None	
US-A- 4463262	31-07-84	None	
FR-A- 2570494	21-03-86	None	
DE-A- 3411186	10-10-85	None	
US-A- 4544441	01-10-85	None	
DE-A- 3240180	03-05-84	None	